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Attorney's Docket No. 760-19

PATENT



IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

Box Patent Application

Assistant Commissioner for Patents
Washington, D.C. 20231

NEW APPLICATION TRANSMITTAL

Transmitted herewith for filing is the patent application of

Inventor(s): **BRODEUR, Christopher, a U.S. Citizen, who address is:**
741 98th Lane N.E., Blaine, MN 55434

For (title): **COMPOSITE TUBULAR PROSTHESES**

CERTIFICATION UNDER 37 CFR 1.10

I hereby certify that this New Application Transmittal and the documents referred to as enclosed herein are being deposited with the United States Postal Service on this date, November 28 , 2000, in an envelope as "Express Mail to Addressee" Mailing Label Number EF117615425US addressed to the Commissioner of Patents and Trademarks, Washington, D.C. 20231.

A.V. Garramone

Name of person mailing paper

Signature of person mailing paper

1. Type of Application

This new application is a(n):

- ☒ Original (nonprovisional) application under
☒ 37 CFR 1.53(b)
- ☐ Divisional of Serial No. _____, filed on _____, under
☐ 37 CFR 1.53(b) ☐ 37 CFR 1.53(d) [CPA]
- ☐ Continuation of Serial No. _____, filed on _____, under
☐ 37 CFR 1.53(b) ☐ 37 CFR 1.53(d) [CPA]
- ☐ Continuation-in-part of Serial No. _____, filed on _____, under
☐ 37 CFR 1.53(b)
- ☐ Design application.
- ☐ Plant application.

2. Benefit of Prior U.S. Application(s) (35 U.S.C. 119(e), 120, or 121)

- ☐ This new application claims the benefit of prior U.S. application(s).
- ☐ Please amend the specification by inserting, before the first line, the following:
- ☐ "This application claims the benefit of U.S. Provisional Application No. _____, filed on _____."
- ☐ "This application is a
☐ continuation
☐ continuation-in-part
☐ divisional
of copending application
☐ Serial No. 08/_____, filed on _____."
☐ International Application No. _____, filed on _____, and
which designated the U.S."
- ☐ A Preliminary Amendment is enclosed amending this application to state the relation of this application to prior applications.
- ☐ The relation of this application to prior applications is stated in the application.

3. 35 U.S.C. 119 Priority Claim for Prior Application

This application, and prior U.S. application(s), including any prior International Application designating the U.S., identified above in item 2, claim(s) priority from one or more foreign applications as follows:

(Country)	(Application No.)	(Filing Date)
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(Country)	(Application No.)	(Filing Date)
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Certified copy(ies) of the application(s) from which priority is claimed:

- ☐ has(have) been filed on _____, in prior application 0 / _____, which was filed on _____.
- ☐ is (are) enclosed.
- ☐ will follow.

4. Papers Enclosed Which are Required to Obtain Application Filing Date under 37 CFR 1.53(b) (Regular) or 37 CFR 1.153 (Design)

11 Pages of specification
5 Pages of claims
1 Pages of Abstract
2 Sheets of drawings
☐ formal
☒ informal

☐ The enclosed drawing(s) include photograph(s), and there is also attached a "Petition to Accept Photograph(s) as Drawings." 37 CFR 1.84(b).

5. Additional Papers Enclosed

- ☐ Preliminary Amendment
- ☐ Information Disclosure Statement (37 CFR 1.98)
- ☐ Form PTO-1449
- ☐ Citations
- ☐ Declaration of Biological Deposit
- ☐ Submission of "Sequence Listing," computer readable copy and/or amendment pertaining thereto for biotechnology invention containing nucleotide and/or amino acid sequence

- ☐ Authorization of Attorney(s) to Accept and Follow Instructions from Representative
- ☐ Special Comments
- ☐ Power of Attorney
- ☐ Other – Change of Assignee Address and Point of Information

6. Declaration or Oath

- ☐ Declaration or Oath is enclosed, executed by (check all applicable boxes):
 - ☐ inventor(s).
 - ☐ legal representative(s) of inventor(s) (37 CFR 1.42 or 1.43).
 - ☐ joint inventor or person showing a proprietary interest on behalf of inventor who refused to sign or cannot be reached.
 - ☐ This transmittal serves as the petition required under 37 CFR 1.47, and the statement required under 37 CFR 1.47 is also enclosed. See item 13 below for fee.
- ☐ A Declaration or Oath was filed on _____ in prior application _____, filed on _____, from which benefit is being claimed for this application under 35 U.S.C. 120 or 121. The subject matter disclosed in the present application is the same as that disclosed in the prior application, and the inventors are the same or less than those named in the prior application. Accordingly, no new Oath or Declaration is required.
 - ☐ A copy of the Oath or Declaration in the prior application is enclosed.
- ☒ A Declaration or Oath is not enclosed.
 - ☐ Application is made by a person authorized under 37 CFR 1.41(c) on behalf of *all* of the above named inventor(s).
- ☐ A Power of Attorney is included in the Declaration or Oath.

7. Language

This new application is written in:

- ☒ English.

- ☐ A non-English language: _____.
- ☐ A verified translation is enclosed (37 CFR 1.52(d)).

8. Assignment

- ☒ An assignment of the invention to **Boston Scientific/SCIMED Life Systems, Inc.**
- ☐ is enclosed. A separate:
- ☐ "Cover Sheet for Assignment (Document) Accompanying New Patent Application" is enclosed.
- ☐ Form PTO-1595 is enclosed.
- ☐ was made in prior application No. _____, filed on _____.
- ☐ A copy of the assignment (and any recordation cover sheet) is enclosed.
- ☒ will follow.

9. Maintenance of Copendency of Prior Application

- ☐ A Petition for Extension of Time and the appropriate fee has been filed and extends the term in the pending prior application until _____.
- ☐ A copy of the petition filed in the prior application is attached.
- ☐ A conditional petition for extension of time is being filed in the pending prior application.
- ☐ A copy of the conditional petition in the prior application is attached.

10. Abandonment of Prior Application

- ☐ Please abandon the prior application at a time while the prior application is pending, or when the petition for extension of time or to revive in that application is granted, and when this application is granted a filing date, so as to make this application copending with said prior application.

11. Petition for Suspension of Prosecution for the Time Necessary to File an Amendment

- ☐ There is provided herewith a Petition to Suspend Prosecution for the Time Necessary to File an Amendment.

12. Fee Calculation (37 CFR 1.16)

A. ☒ Regular application (37 CFR 1.16(a)) Basic Fee \$ 710.00

FEEES FOR CLAIMS AS FILED

Number filed	Number extra	Rate		
Total Claims (37 CFR 1.16(c))	18 - 20 =	X \$ 18.00	=	\$.00
Independent Claims (37 CFR 1.16(b))	4 - 3 = 1	X \$ 80.00	=	\$ 80.00
Multiple Dependent Claims (37 CFR 1.16(d))		+ \$260.00	=	\$

Fee Calculation for Extra Claims \$ 80.00

- ☐ Amendment canceling extra claims enclosed.
☐ Amendment deleting multiple-dependencies enclosed.

B. ☐ Design application (37 CFR 1.16(f)) Filing Fee \$330.00

C. ☐ Plant application (37 CFR 1.16(g)) Filing Fee \$540.00

Total Filing Fee Calculation \$ 790.00

13. Request for International-Type Search (37 CFR 1.104(d))

- ☐ Please prepare an international-type search report for this application at the time national examination on the merits takes place. See item 15 for fee.

14. Small Entity Statement(s)

- ☐ A Verified Statement that this is a filing by a small entity under 37 CFR 1.9 and 1.27;
☐ is enclosed.
☐ will follow.

- ☐ Status as a small entity was claimed in prior application 0 / _____, filed on _____, from which benefit is being claimed for this application under:

- ☐ 35 U.S.C. 119(e),
☐ 35 U.S.C. 120,
☐ 35 U.S.C. 121,
☐ 35 U.S.C. 365(c),

and which status as a small entity is still proper and desired.

☐ A copy of the verified statement in the prior application is enclosed.

Filing Fee Calculation (50% of A, B, or C above) \$ _____

15. Fee Payment Being Made at This Time

☐ Not enclosed. No filing fee is to be paid at this time.

☒ Enclosed:

<input checked="" type="checkbox"/>	Basic filing fee (Item 12 or 14 above)	\$ <u>790.00</u>
<input type="checkbox"/>	Fee for recording Assignment (\$40.00 (37 CFR 1.21(h)))	\$ _____
<input type="checkbox"/>	Petition fee for filing by other than all of the inventors or person on behalf of the inventor where inventor refused to sign or cannot be reached. (\$130.00 (37 CFR 1.47 and 1.17(h)))	\$ _____
<input type="checkbox"/>	Fee for processing an application having a specification in a non-English language. (\$130.00 (37 CFR 1.52(d) and 1.17(k)))	\$ _____
<input type="checkbox"/>	Processing and retention fee (\$130.00 (37 CFR 1.53(d) and 1.21(l)))	\$ _____
<input type="checkbox"/>	Fee for international-type search report (\$40.00 (37 CFR 1.21(e)))	\$ _____
	Total fees enclosed	\$ <u>790.00</u>

16. Method of Payment of Fees

☒ Check in the amount of \$ 790.00.

☐ Charge Deposit Account No. 08-2461 in the amount of \$ _____.
A duplicate of this transmittal is enclosed.

17. Authorization to Charge Additional Fees

☒ The Commissioner is hereby authorized to charge the following additional fees by this paper and during the entire pendency of this application to Deposit Acc't No. 08-2461:

☒ 37 CFR 1.16(a), (f), or (g) (filing fees)

☒ 37 CFR 1.16(b), (c), and (d) (presentation of extra claims)

☐ 37 CFR 1.16(e) (surcharge for filing the basic fee and/or declaration at a date later than the filing date of the application)

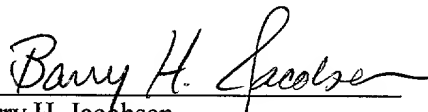
☐ 37 CFR 1.17 (application processing fees)

A duplicate of this transmittal is enclosed.

18. Instructions as to Overpayment

☒ Credit Deposit Account 08-2461.

☐ Refund.


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COMPOSITE TUBULAR PROSTHESES**FIELD OF INVENTION:**

The present invention relates generally to a tubular implantable prosthesis formed of porous expanded polytetrafluoroethylene. More particularly, the present invention relates to a composite, multi-layered endoprosthesis having increased axial and circumferential compliance.

BACKGROUND OF RELATED TECHNOLOGY:

An intraluminal prosthesis is a medical device used in the treatment of diseased blood vessels. An intraluminal prosthesis is typically used to repair, replace, or otherwise correct a diseased or damaged blood vessel. An artery or vein may be diseased in a variety of different ways. The prosthesis may therefore be used to prevent or treat a wide variety of defects such as stenosis of the vessel, thrombosis, occlusion, or an aneurysm.

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One type of intraluminal prosthesis used in the repair of diseases in various body vessels is a stent. A stent is a generally longitudinal tubular device formed of biocompatible material which is useful to open and support various lumens in the body. For example, stents may be used in the vascular system, urogenital tract and bile duct, as well as in a variety of other applications in the body. Endovascular stents have become widely used for the treatment of stenosis, strictures, and

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aneurysms in various blood vessels. These devices are implanted within the vessel to open and/or reinforce collapsing or partially occluded sections of the vessel.

Stents are generally open-ended and are radially expandable between a generally unexpanded insertion diameter and an expanded implantation diameter which is greater than the unexpanded insertion diameter. Stents are often flexible in configuration, which allows them to be inserted through and conform to tortuous pathways in the blood vessel. The stent is generally inserted in a radially compressed state and expanded either through a self-expanding mechanism, or through the use of balloon catheters.

A graft is another commonly known type of intraluminal prosthesis which is used to repair and replace various body vessels. A graft provides a lumen through which blood may flow. Grafts are typically tubular devices which may be formed of a variety of materials, including textiles, and non-textile materials. One type of particularly useful non-textile material for an implantable intraluminal prosthesis is polytetrafluoroethylene (PTFE). PTFE exhibits superior biocompatibility and low thrombogenicity, which makes it particularly useful as vascular graft material in the repair or replacement of blood vessels. In vascular applications, grafts are often manufactured from expanded polytetrafluoroethylene (ePTFE) tubes. These tubes have a microporous structure which allows natural tissue ingrowth and cell endothelialization once implanted in the vascular system. This contributes to long term healing and patency of the graft.

Grafts formed of ePTFE have a fibrous state which is defined by interspaced nodes interconnected by elongated fibrils. The spaces between the node surfaces that

is spanned by the fibrils is defined as the internodal distance (IND). Porosity of a graft is generally described using IND. In order to have proper tissue ingrowth and cell endothelization, grafts must have sufficient porosity obtained through expansion.

When the term expanded is used to describe PTFE, it is intended to describe PTFE
5 which has been stretched, in accordance with techniques which increase the IND and concomitantly porosity. The stretching may be uni-axial, bi-axial, or multi-axial. The space between the nodes is occupied by the stretched fibrils.

Properties such as tensile strength, tear strength and circumferential (hoop)
10 strength are all dependent on the expansion process. Expanding the film by stretching it in two directions that are substantially perpendicular to each other, for example longitudinally and transversely, creates a biaxially oriented material. Films having multi-axially-oriented fibrils may also be made by expanding the film in more than two directions. Porous ePTFE grafts have their greatest strength in directions
15 parallel to the orientation of their fibrils.

Longitudinal compliance is of particular importance to an intraluminal prosthesis that is delivered through tortuous pathways of a blood vessel to the implantation site where it is expanded. Conventional PTFE containing grafts exhibit
20 low longitudinal compliance and as such have decreased flexibility, which makes intraluminal delivery more difficult. Additionally, conventional PTFE containing grafts may fail at the outer circumference when the PTFE is at a stretch limit such as at a bend point around a corner.

Accordingly, it is desirable to provide a PTFE graft that has high axial and longitudinal compliance. Additionally, it is desirable to provide a PTFE that has a low failure rate at points where the PTFE outer circumferential is at a stretch limit.

5 SUMMARY OF THE INVENTION:

The present invention is directed towards an implantable composite tubular prosthesis. The composite has three layers; a first tubular ePTFE body, a second perimetrically non-continuous tubular body, and a circumferentially support structure between the tubular bodies. The first tubular body may be the inner tubular body and
10 the second tubular body may be the outer tubular body. Alternatively, the first tubular body may be the outer tubular body and the second tubular body may be the inner tubular body. The outer layer may be ePTFE or PTFE.

More particularly, the present invention provides a composite implantable
15 tubular prosthesis which has a first substantially continuous ePTFE tubular body and a second tubular body. A circumferentially deformable support structure is interposed between the two tubular PTFE bodies. The second tubular body is formed of a plurality of elongate PTFE strips. The strips are arranged longitudinally in a non-over-lapping relationship and secured to the first body desirably through and
20 about the distensible support structure. Use of the non-overlapping strips of the second tubular body provide axial and circumferential compliance to the prosthesis. In an alternative embodiment, the inner tubular body may be formed of non-overlapping ePTFE strips, overlapping the discontinuities in the outer tubular body.

The present invention also provides an implantable composite intraluminal prosthesis having a first perimetrically non-continuous polytetrafluoroethylene tubular inner body; a second perimetrically non-continuous outer tubular body; and a circumferentially deformable support structure interposed between the inner and
5 outer tubular bodies. Both the outer tubular body and the inner tubular body are formed of polytetrafluoroethylene strips, having a longitudinal length greater than its width, and the strips within each tubular body arranged in non-over-lapping relationship, with the strips of the inner tubular body overlapping the discontinuities of the outer tubular body, and secured in the overlap, whereby axial and
10 circumferential compliance is provided to the prosthesis.

Another embodiment of the present invention provides for a method of providing axial and circumferential compliance to an intraluminal prosthesis stent/graft composite including providing a substantially continuous
15 polytetrafluoroethylene tubular first body; positioning a deformable support structure over the tubular first body; positioning PTFE strip components in non-overlapping relationship, lengthwise along the length of the first body and support structure to form a tubularly shaped second body; and attaching the strips of the second body to the first body.

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A further embodiment of the present invention provides for a method of providing axial and circumferential compliance to an intraluminal prosthesis stent/graft composite including positioning PTFE strip components, having a length greater than their width, lengthwise along a mandrel, in non-overlapping relationship,
25 to form a circumferentially non-continuous polytetrafluoroethylene tubular first

body; positioning a deformable support structure over the first body; positioning PTFE strip components, lengthwise along the longitudinal axis of the first body, in non-overlapping relationship but overlapping the discontinuities of the first body to form a second body; and securing the second body to the first body to form the prosthesis.

BRIEF DESCRIPTION OF THE DRAWINGS

Figure 1 is an exploded perspective view showing an implantable composite tubular prosthesis according to the present invention, illustrating first body 1, support structure 3, and second body 4.

Figures 2-4 are exploded perspective views of alternative structures of the prosthesis.

DETAILED DESCRIPTION OF THE INVENTION:

The prosthesis of one desired embodiment of the present invention is a composite implantable intraluminal prosthesis which is particularly suited for use as a vascular graft. As shown in Figure 1, this composite prosthesis includes a multi-layer graft structure with a circumferentially deformable support structure 3 interposed between an ePTFE first tubular body 1, and non-continuous second body 4, formed of PTFE components. The present description is meant to describe all the desired embodiments, and is not meant to limit the invention in any way.

As shown in Figure 1, first body 1 may be a substantially continuous tubular structure, formed by various methods such as by forming a tube with a sheet, a

spirally wrapped strip or extruding a tube. For example, if a sheet is used, the first body 1 can be formed by wrapping the sheet around a longitudinal axis, such as around a mandrel (not shown), to form a tubular body 1' with a longitudinal seam 2'.

Continuous, as used herein, refers to a tubular structure whose surface extends
5 substantially uninterrupted throughout the longitudinal length thereof. In the case of an extruded tube, the tubular structure is completely uninterrupted. A substantially uninterrupted tubular structure exhibits enhanced strength and sealing properties when used as a vascular graft. Furthermore, the first tubular body may consist of one single layer or it may consist of multiple layers of the PTFE sheet around the
10 longitudinal axial to create a multi-layer inner tube. The first body may be the inside tubular body and the second body may be the outer tubular body. Alternatively, the first body may be the outer tubular body and the second body may be the inner tubular body.

15 As shown in Figure 2, first tubular body 5 may be formed of longitudinal strips or components. Alternatively, the first tubular body may be formed of one or more helically wound strips or components 8 and 11 as shown in Figures 3 and 4.

As shown herein, the second tubular body shown in Figures 1-4 form
20 perimetrically non-continuous bodies from PTFE components tubularly assembled. Non-continuous, as used herein, refers to a tubular structure which is not substantially uninterrupted along its length. The non-continuous structure of the outer tubular body provides the composite prosthesis with enhanced radial and axial compliance. The radial and axial compliance can, in fact, be varied with the different
25 outer PTFE bodies which may be used, as may be suitable particularly for the use of

the intraluminal prosthesis. The non-continuous second body 4 is formed of PTFE components which may be, for example, coated, extruded, woven or braided. As seen in Figures 2 and 3, the second body 7 and 10 may be individual strips which may be non-continuous having longitudinally arranged segments.

5

In a desired embodiment, the PTFE components forming the second tubular body are expanded PTFE (ePTFE) strips. Generally ePTFE strips are stretched in the longitudinal direction of the strip. When two or more components are combined to form the outer tubular body, the resultant tubular body possesses a biaxial, or multi-axial resultant orientation in the aggregate. Because ePTFE exhibits increased strength in the direction of its stretching, the ePTFE tubularly assembled prosthesis exhibits the advantage of the increased strength of a biaxial or multi-axial stretched film, but also exhibits longitudinal compliance because of the presence of a non-continuous tubular surface.

15

When both tubular bodies are formed of perimetrically non-continuous strips, as in Figure 2, the two tubular bodies desirably have radially overlapping portions which may be adhered to one another to form the composite prosthesis. As shown in Figure 4, continuous longitudinal strips 11 and 13 may be sinusoidal, extending in a wave pattern down the length of the tubular bodies.

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The first tubular layer may be bonded to the second tubular layer through spaces in the open wall of the stent. The bonding may be effectuated with the use of an adhesive, or by adhering the layers together without an adhesive. Bonding of the PTFE layers without an adhesive may take place by such methods as thermally

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bonding, also known as laminating. Furthermore, the stent may be adhered to the first tubular layer, the second tubular layer, or both. Similarly, such adherence may take place with or without the use of an adhesive. The components may be fully or partially bonded.

5

The present invention also contemplates that a deformable support member or stent is used with the prosthesis of the present invention to provide a composite intraluminal prosthesis. A deformable support member is desirably a stent which is positioned between the first and second tubular bodies. Stent 3 and 6 is a length of
10 wire distensible material that has longitudinally adjacent waves being nested along the length of the tubular body, as shown in Figures 1 and 2. Overlying the deformable support member is perimetrically non-continuous second body 4, having longitudinally arranged strips.

15 Various stent types and stent constructions may be employed in the invention. Useful stents include, without limitation, self-expanding stents and balloon expandable stents. The stents may be capable of radially contracting, as well, and in this sense can be best described as radially or circumferentially distensible or deformable. Self-expanding stents include those that have a spring-like action which
20 causes the stent to radially expand, or stents which expand due to the memory properties of the stent material for a particular configuration at a certain temperature. Nitinol is one material which has the ability to perform well while both in spring-like mode, as well as in a memory mode based on temperature. Other materials are of course contemplated, such as stainless steel, platinum, gold, titanium and other
25 biocompatible metals, as well as polymeric stents.

The configuration of the stent may be of any geometry. As shown in Figures 1 and 2, useful wire stents 3 and 6 include longitudinally adjacent waves being nested along the length of the tubular body with the peaks of the longitudinally nested waves linearly aligned. The deformable support structure may include a plurality of spaced apart circumferentially extending bands. Tubular stents 9 and 12, useful in the present invention, also include those formed by etching or cutting a pattern from a tube as shown in Figures 3 and 4. Such stents are often referred to as slotted stents. Furthermore, stents may be formed by etching a pattern into a material or mold and depositing stent material in the pattern, such as by chemical vapor deposition or the like.

PTFE components that can be used for the tubular bodies may be selected from the group consisting of yarns, fibers, sheets and tubes. The tubular bodies of the present invention may be wrapped by various methods. Useful wrap methods include a segmented tube, segmented helical, helical, longitudinal strip, segmented longitudinal helical and combinations thereof.

Sealants that may be used in the prosthesis include fluorinated ethylene propylene (FEP), polyurethane, and silicone. Additional sealants include biological materials such as collagen, and hydrogels, polymethylmethacrylate, polyamide, and polyurethane-polycarbonate. Elastomers as sealants will have less impact on flexibility. A suitable sealant provides a substantially sealed outer tube without significantly reducing longitudinal and axial compliance.

Although illustrative embodiments of the present invention have been described herein with reference to the accompanying drawings, it is to be understood that the invention is not limited to those precise embodiments, and that various other changes and modifications may be effected therein by one skilled in the art without
5 departing from the scope or spirit of the invention.

WHAT IS CLAIMED IS:

1. An implantable composite tubular prosthesis comprising:
a first substantially continuous PTFE tubular body;
a second perimetrically non-continuous tubular body; and
a circumferentially deformable support structure interposed between said
5 tubular bodies,
said second tubular body being formed of a plurality of elongate
polytetrafluoroethylene strips, said strips secured to the first tubular body, arranged
longitudinal in non-over-lapping relationship, whereby axial and radial compliance
is provided to said prosthesis.
2. The composite tubular prosthesis according to claim 1, wherein said
first tubular body is an inner tubular body and said second tubular body is an outer
tubular body of said prosthesis.
3. The composite tubular prosthesis according to claim 1, wherein said
first tubular body is an outer tubular body and said second tubular body is an inner
tubular body of said prosthesis.
4. The composite tubular prosthesis according to claim 1, wherein the
PTFE of said first body is expanded PTFE.
5. The composite tubular prosthesis according to claim 1, wherein said
deformable support structure is a stent.

6. The composite intraluminal prosthesis according to claim 1, wherein the deformable support structure comprises a plurality of spaced apart circumferentially extending bands.

7. The composite tubular prosthesis according to claim 1, wherein said PTFE second tubular body is wrapped by a material selected from the group consisting of yarns, fibers, sheets and tubes.

8. The composite tubular prosthesis according to claim 1, wherein said strips of said second tubular body is a wrap configuration secured to said first body; said wrap configuration selected from the group consisting of a segmented tube, a segmented helical wrap, a continuous non-overlapping helical strip, one or more longitudinal oriented strips and a plurality of segmented longitudinal helical strips.

9. The composite intraluminal prosthesis according to claim 1, wherein the substantially continuous body is formed of a sheet or spirally wrapped strip.

10. The composite intraluminal prosthesis as in claim 1, wherein the first tubular body is an extruded PTFE tube.

11. The composite intraluminal prosthesis as in claim 1, wherein the PTFE of said second body is ePTFE.

12. The composite intraluminal prosthesis according to claim 1, wherein the deformable support structure is a wire stent with longitudinally adjacent waves being nested along the length of the tubular body and peaks of said longitudinally nested waves are linearly aligned.

13. The composite intraluminal prosthesis according to claim 1, wherein the first body is secured to said second body by thermal bonding.

14. The composite intraluminal prosthesis according to claim 1, wherein the second polytetrafluoroethylene body comprises segments of polytetrafluoroethylene strips.

15. The composite intraluminal prosthesis according to claim 1, wherein said continuous polytetrafluoroethylene tubular first body is comprised of a sheet of expanded polytetrafluoroethylene formed into a tubular shape by wrapping said sheet about a longitudinal axis.

16. An implantable composite intraluminal prosthesis comprising:
a first perimetrically non-continuous polytetrafluoroethylene tubular inner
body;

a second perimetrically non-continuous polytetrafluorethylene outer tubular
5 body, and

a circumferentially deformable support structure interposed between the inner
and outer tubular bodies,

both said outer tubular body and said inner tubular body being formed of
polytetrafluoroethylene strips, having a longitudinal length greater than its width, and
10 said strips within each tubular body arranged in non-over-lapping relationship, with
the strips of the inner tubular body overlapping the discontinuities of the outer
tubular body, and secured in the overlap, whereby axial and circumferential
compliance is provided to said prosthesis.

17. A method of providing axial and circumferential compliance to an
intraluminal prosthesis stent/graft composite comprising:

- a) providing a first substantially continuous polytetrafluoroethylene
tubular body;
- 5 b) positioning a deformable support structure over the tubular first body;
- c) positioning PTFE strip components in non-overlapping relationship,
lengthwise along the length of the first body and support structure to
form a tubularly shaped second body; and
- d) attaching the strips of the second body to the first body.

18. A method of providing axial and circumferential compliance to an intraluminal prosthesis stent/graft composite comprising:

- 5 a) positioning PTFE strip components, having a length greater than their width, lengthwise along a mandrel, in non-overlapping relationship, to form a circumferentially non-continuous polytetrafluoroethylene tubular first body;
- b) positioning a deformable support structure over said first body;
- 10 c) positioning PTFE strip components, lengthwise along the longitudinal axis of said inner body, in non-overlapping relationship but overlapping the discontinuities of the first body to form a second body; and
- d) securing said second body to the first body to form said prosthesis.

COMPOSITE TUBULAR PROSTHESES

ABSTRACT OF THE DISCLOSURE:

A tubular implantable prosthesis is formed of porous expanded polytetrafluoroethylene. The tubular prosthesis includes a substantially continuous ePTFE tubular first body and perimetrically non-continuous second tubular body. A circumferentially deformable support structure is interposed between the inner and outer tubular bodies. The second tubular body is formed of a plurality of elongate PTFE strips. The strips are secured to the first body and arranged longitudinally in a non-overlapping relationship. The prosthesis provides for both axial and radial compliance.

Figure 1

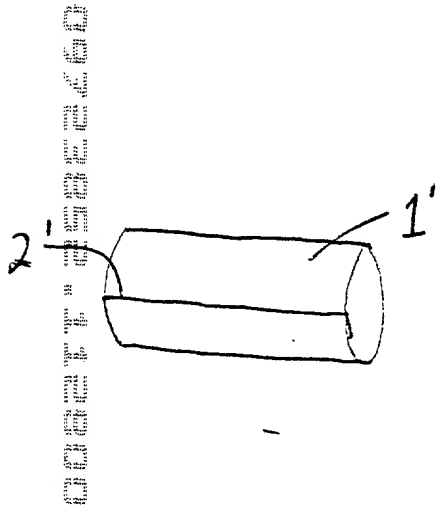
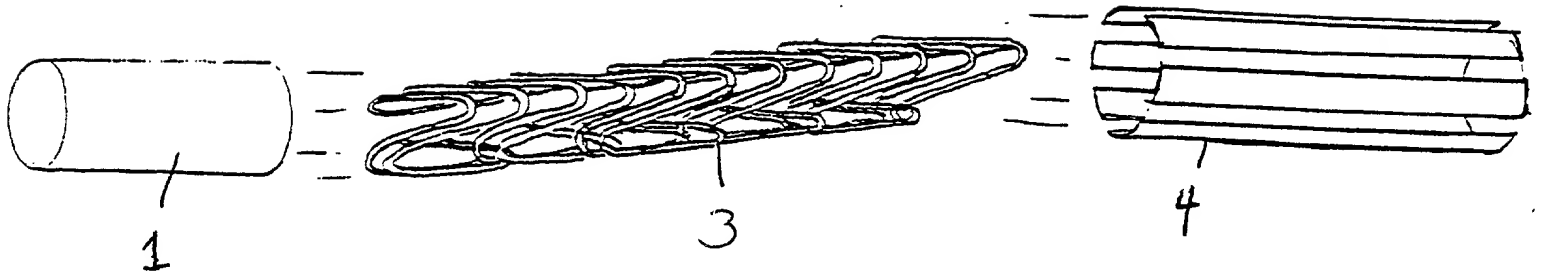


Figure 2

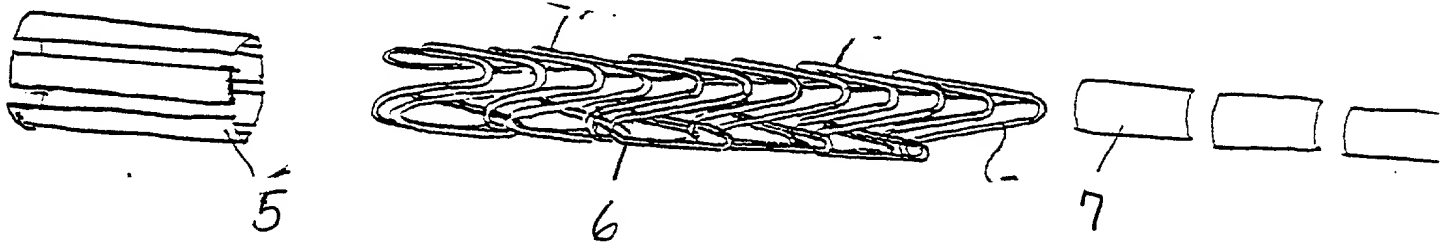


Figure 3

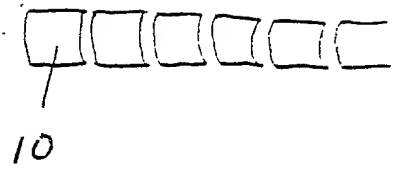
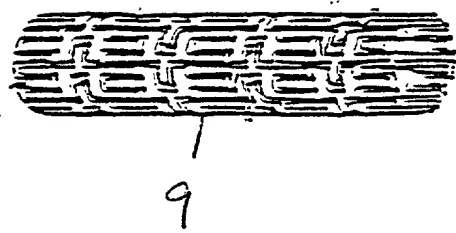
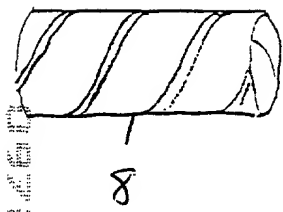


Figure 4

